

## Research Paper

# Dual Receptor Recognizing Cell Penetrating Peptide for Selective Targeting, Efficient Intratumoral Diffusion and Synthesized Anti-Glioma Therapy

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## Abstract

Cell penetrating peptides (CPPs) were widely used for drug delivery to tumor. However, the nonselective *in vivo* penetration greatly limited the application of CPPs-mediated drug delivery systems. And the treatment of malignant tumors is usually followed by poor prognosis and relapse due to the existence of extravascular core regions of tumor. Thus it is important to endue selective targeting and stronger intratumoral diffusion abilities to CPPs. In this study, an RGD reverse sequence dGR was conjugated to a CPP octa-arginine to form a CendR (R/KXXR/K) motif contained tandem peptide R8-dGR (RRRRRRRRdGR) which could bind to both integrin  $\alpha_3\beta_3$  and neuropilin-1 receptors. The dual receptor recognizing peptide R8-dGR displayed increased cellular uptake and efficient penetration ability into glioma spheroids *in vitro*. The following *in vivo* studies indicated the active targeting and intratumoral diffusion capabilities of R8-dGR modified liposomes. When paclitaxel was loaded in the liposomes, PTX-R8-dGR-Lip induced the strongest anti-proliferation effect on both tumor cells and cancer stem cells, and inhibited the formation of vasculogenic mimicry channels *in vitro*. Finally, the R8-dGR liposomal drug delivery system prolonged the medium survival time of intracranial C6 bearing mice by 2.1-fold compared to the untreated group, and achieved an exhaustive anti-glioma therapy including anti-tumor cells, anti-vasculogenic mimicry and anti-brain cancer stem cells. To sum up, all the results demonstrated that R8-dGR was an ideal dual receptor recognizing CPP with selective glioma targeting and efficient intratumoral diffusion, which could be further used to equip drug delivery system for effective glioma therapy.

Key words: Cell penetrating peptides, Tumor penetration, C-end Rule, Glioma targeting, Anti-glioma

## Introduction

Cell penetrating peptides (CPPs) are a class of diverse short peptides which can break through various bio-barriers including blood-brain barrier (BBB), intestine wall, retina and neurons[1, 2]. In recent decade, CPPs were widely used for tumor delivery of nano drug carriers due to their ability of overwhelming cell penetration and internalization[3-5]. Nevertheless, the application of CPP-mediated drug carriers

was greatly limited because of the nonselectivity of CPPs *in vivo*[2]. Besides, it is difficult for nanocarriers to deliver deep into the hypoxic and necrotic regions of solid tumors due to the elevated interstitial fluid pressure (IFP), abnormal vasculature and relative high cell density[6-9]. Although CPPs would benefit intratumoral diffusion of drug delivery systems in some degree, the penetration efficiency into the core

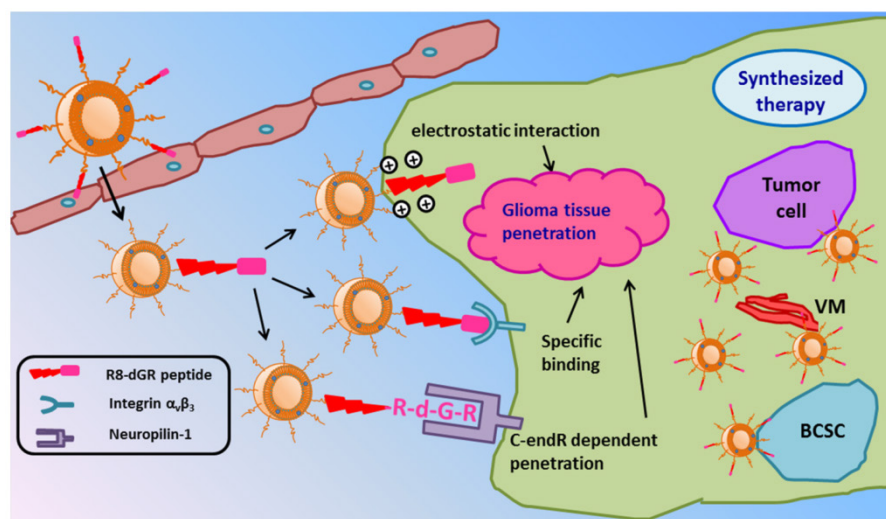
areas distant from the vascular bed was still limited and needed to be further improved. And this improvement would significantly enhance the anti-tumor therapeutic effect[10]. Therefore, the structural modification of CPPs focused on enhancing the selective targeting and intratumoral penetrating abilities is necessary.

Erkki Ruoslahti's group identified that an exposed R/KXXR/K C-terminal sequence of peptide could specifically recognize a cell surface receptor neuropilin-1 (NRP-1) which plays an important role in angiogenesis and regulation of vascular permeability[11]. NRP-1 was found overexpressed on both endothelial cells and tumor cells[12, 13], thus this kind of C-terminal motif could efficiently mediate cell, vascular and tissue penetration by binding to NRP-1[11]. This phenomenon was termed C-end Rule (CendR) and proved in many researches[14-17]. In the previous study, our group had reported that a tandem peptide by combination of R8 and c(RGDfK) could overcome the non-selective property of CPPs, thus achieve a successful BBB transporting and glioma targeting effect[18]. Based on this and in order to further enhance the glioma tissue penetrating ability, we designed another dual receptor recognizing cell penetrating peptide herein with a sequence of RRRRRRRRdGR (R8-dGR, lower case letter represents D-amino acid residue). By connecting an RGD reverse sequence dGR to a CPP octa-arginine, this peptide was endowed with selective targeting property by recognizing both integrin  $\alpha_v\beta_3$  and NRP-1 receptors, and could undergo a CendR based intratumoral penetrating process. This is the first time to report one CPP-based peptide which could recognize two kinds

of receptors on tumor cells, and the tumor targeting and tissue penetrating capabilities could both be enhanced.

Recent researches proved that aggressive tumors like malignant glioma was highly correlated with the formation of vasculogenic mimicry (VM) and brain cancer stem cells (BCSCs)[19-22]. VM is non-endothelial tumor cell-lined microvascular channel which could transport nutrients independent of endothelial blood vessels[23]. Researchers suggested that VM provided an alternative vascularization pathway to keep tumor cells nourished in hypoxic and ischemic microenvironment[24]. Meanwhile, during the tumorigenesis of glioma, a few subpopulations of glioma cancer cells expressing CD133 are enriched to form cancer stem cells and exhibit greater tumorigenic potential than normal cancer cells[25]. BCSCs are commonly tolerated to chemotherapeutics and possess the capabilities of self-renewal and proliferation, which inevitably lead to the relapse of glioma[26]. Therefore, the synthesized anti-glioma effect with combined treatment of tumor cells, VM and BCSCs is important.

In this study, we hypothesized paclitaxel (PTX) loaded R8-dGR modified liposomes (PTX-R8-dGR-Lip) as potential anti-glioma drug delivery systems. As illustrated in Fig. 1, PTX-R8-dGR-Lip could transport across the BBB through integrin-binding and CPP mediated penetrating. After accumulated in the glioma foci, R8-dGR could induce an efficient glioma tissue penetrating process *via* the synergetic effect of three pathways including electrostatic interaction, specific binding with integrin  $\alpha_v\beta_3$  and CendR dependent penetration.



**Fig. 1.** Schematic illustration of PTX-R8-dGR-Lip. After transporting across the BBB and accumulating in glioma foci, liposomes could achieve an efficient synergetic glioma tissue penetration through three pathways and accomplish a synthesized anti-glioma therapy by combined treatment of tumor cells, VM and BCSCs.

Therefore, PTX-loaded liposomes could be delivered to the inner region of glioma and exhibit a synthesized anti-glioma therapeutic effect by combined treatment of tumor cells, vasculogenic mimicry and brain cancer stem cells. We investigated the integrin  $\alpha_v\beta_3$  and NRP-1 recognizing, glioma spheroids penetrating and BBB model transporting abilities of R8-dGR *in vitro*, studied the glioma targeting properties of modified liposomes *in vivo*, and carried out a synthesized anti-glioma evaluation by investigating the inhibition effect of different PTX-Lip on C6 cells, C6 VM channels and C6 stem cells both *in vitro* and *in vivo*.

## Materials and methods

### Materials

R8-dGR, R8-RGD and R8-EGR peptide with an N-terminal cysteine (Cys-RRRRRRRRdGR, Cys-RRRRRRRRRGD and Cys-RRRRRRRRREGR) were synthesized according to the standard solid phase peptide synthesis by Chinapeptides Co. Ltd. (Shanghai, China). R8 peptide with an N-terminal cysteine (Cys-RRRRRRRR) was synthesized according to the standard solid phase peptide synthesis by Chengdu Kai Jie Bio-pharmaceutical Co. Ltd. (Chengdu, China). Soybean phospholipids (SPC) were purchased from Shanghai Taiwei Chemical Company (Shanghai, China). Cholesterol was purchased from Chengdu Kelong Chemical Company (Chengdu, China). 1, 2-dioleoyl-sn-glycero-3-phosphoethanolamine-N-(carboxyfluorescein) (CFPE), were obtained from Avanti Polar Lipids (USA). DSPE-PEG<sub>2000</sub> and DSPE-PEG<sub>2000</sub>-Mal were purchased from Shanghai Advanced Vehicle Technology (AVT) L.T.D. Company (Shanghai, China). Paclitaxel was purchased from AP Pharmaceutical Co. Ltd. (Chongqing, China). The recombinant mouse integrin  $\alpha_3\beta_3$  was purchased from R&D systems (U.S.A). Rabbit anti-mouse  $\beta_3$  integrin primary antibodies were purchased from Epitomics, Abcam (California, USA). Rabbit anti-Neuropilin 1, anti-CD133 anti-GAPDH and anti-ZO-1 antibodies were purchased from Boster (China). Horseradish peroxidase (HRP) -labeled goat anti-rabbit secondary antibodies was purchased from ZSGB-BIO (Beijing, China). 1, 10-dioctadecyl-3, 3, 30-tetramethylindodicarbocyanine, 4-chlorobenzenesulfonate salt (DiD) were purchased from Biotium (USA). Annexin V-FITC/PI apoptosis detection kit was purchased from KeyGEN Biotech (China). BD Matrigel™ Basement Membrane Matrix was purchased from BD Biosciences (Franklin Lakes, NJ). Millicell Hanging Cell Culture Inserts were purchased from Millipore (USA). The other chemicals were obtained from commercial sources.

Balb/c mice were purchased from West China animal center of Sichuan University (Sichuan, China). All animal experiments were approved by the Experiment Animal Administrative Committee of Sichuan University.

### Synthesis of different materials

Peptide conjugated DSPE-PEG<sub>2000</sub> materials (DSPE-PEG<sub>2000</sub>-R8-dGR, DSPE-PEG<sub>2000</sub>-R8-RGD, DSPE-PEG<sub>2000</sub>-R8-EGR and DSPE-PEG<sub>2000</sub>-R8) were synthesized through Michael addition reaction. Briefly, DSPE-PEG<sub>2000</sub>-Mal and Cys-R8-dGR (or Cys-R8-RGD, Cys-R8-EGR, Cys-R8) were dissolved with a molar ratio of 1: 1.5 in chloroform/methanol

(v/v = 2: 1) containing triethylamine as a catalyst. The mixture was then allowed to react for 24 h in darkness under room temperature. After the disappearance of DSPE-PEG<sub>2000</sub>-Mal was confirmed by thin layer chromatography, the organic solvent was evaporated by rotary evaporation and the residue was redissolved by chloroform. The solution was then filtered for purification and the filtrate was evaporated again to obtain the production. All the DSPE-PEG<sub>2000</sub> materials were stored under -20 °C until used. The synthesis of DSPE-PEG<sub>2000</sub>-R8-dGR, DSPE-PEG<sub>2000</sub>-R8-RGD and DSPE-PEG<sub>2000</sub>-R8 was confirmed by mass spectrometry (autoflex III smartbeam, Bruker, USA) while that of DSPE-PEG<sub>2000</sub>-R8-EGR was detected by MS (Q-TOF Premier, Waters, USA). All the DSPE-PEG<sub>2000</sub>-peptide conjugates were analyzed by HPLC (Agilent, USA). The mobile phase was a 30:70 (V/V) mixture of acetonitrile and water containing 0.1% trifluoroacetic acid. The samples were detected at 220 nm.

### Preparation and characterization of liposomes

All the liposomes were prepared by thin film hydration method. In brief, SPC, cholesterol and DSPE-PEG<sub>2000</sub> (molar ratio = 62: 33:5) were dissolved in chloroform. Then the organic solvent was evaporated by rotary evaporation. The formed lipid film was hydrated in phosphate buffered saline (pH 7.4) for 20 min under 37 °C. Then the solution was intermittently sonicated by a probe sonicator at 80 W for 80 s to form PEGylated liposomes (PEG-Lip). R8-dGR modified liposomes (R8-dGR-Lip), R8-RGD modified liposomes (R8-RGD-Lip), R8-EGR modified liposomes (R8-EGR-Lip) and R8 modified liposomes (R8-Lip) were prepared by a similar method with 0.8% of DSPE-PEG<sub>2000</sub> in PEG-Lip being replaced by equal amounts of DSPE-PEG<sub>2000</sub>-R8-dGR, DSPE-PEG<sub>2000</sub>-R8-RGD, DSPE-PEG<sub>2000</sub>-R8-EGR and DSPE-PEG<sub>2000</sub>-R8, respectively. PTX-loaded liposomes (PTX-Lip), CFPE-labeled liposomes and DiD-loaded liposomes were prepared with appropriate amount of PTX, CFPE or DiD added to the lipid solution prior to the evaporation respectively.

The entrapment efficiency of PTX was determined by HPLC (Agilent, USA). Malvern Zetasizer Nano ZS90 (Malvern Instruments Ltd., UK) was used to determine the mean size and zeta potential of different groups of liposomes. Serum stability of liposomes was evaluated by monitoring the turbidity variations of liposomes incubated with FBS. Liposomes were mixed with equal volume of FBS and then incubated under 37 °C with gentle oscillating for 48 h. At predetermined time points, the transmittance of the mixture was measured by a microplate reader (Thermo Scientific Varioskan Flash, USA) at 750 nm.

*In vitro* drug release study was performed by a dialysis method using PBS (pH 7.4) containing 0.1% Tween 80 (v/v) as the release media. 0.5 mL PTX-loaded liposomes or free PTX were placed into cellulose acetate dialysis tubes (MWCO 8-14 kDa) and immersed in 50 mL release medium, followed by gently shaking under 37 °C. Then 0.1 mL release media was sampled and replaced with equal volume of fresh release media at predetermined time points. The amount of released PTX was analyzed by HPLC.

Surface plasmon resonance (SPR) technology was performed to evaluate the interaction efficiency between liposomes and integrin. A biacore T200 instrument (Biacore T200, GE Healthcare) was used here. Integrin  $\alpha_v\beta_3$  was linked on CM5 sensor chips by amine coupling. After the baseline was stable, different liposomes were injected over the sensor chips for 30 s at a flow rate of 10  $\mu$ L/min. The response signals were then recorded and analyzed. Before each injection, the phosphate buffer was used to wash the samples off the sensor chip.

### Cell culture

C6 cells (murine glioma cells), bEnd.3 cells (murine brain endothelial cells) and Hela cells (human cervical carcinoma cells) were cultured in DMEM medium (Gibco) supplement with 10% fetal bovine serum (FBS), 100 U/mL penicillin and 100  $\mu$ g/mL streptomycin at 37 °C in a humidified 5% CO<sub>2</sub> atmosphere.

### Receptor expression level

The expression level of NRP-1 and integrin  $\beta_3$  on C6 cells, bEnd.3 cells and Hela cells were measured using western blot studies. The total protein samples of different kinds of cells were extracted, separated on 10% SDS-PAGE and transferred to polyvinylidene difluoride membranes. The membranes were incubated with Rabbit anti-Neuropilin-1, anti-integrin  $\beta_3$  or anti-GAPDH primary antibodies. All the membranes were then incubated with HRP-labeled goat anti-rabbit secondary antibodies and monitored by Immobilon Western HRP Substrate (Millipore, USA) on a Bio-Rad ChemiDoc MP System (Bio-Rad Laboratories, USA).

### Cellular uptake study

The liposomal cellular uptake was evaluated on C6, bEnd.3 and Hela cells. For quantitative analysis, all kinds of cells were plated in 6-well plates at a density of  $5 \times 10^5$  cells per well. After incubation for 24 h, different CFPE-labeled liposomes were added into the plates for 4 h incubation. Then the cells were washed twice with cold PBS, trypsinized, resuspended in 0.5 mL PBS and finally analyzed by a flow cytometer (Cytomics FC 500, Beckman Coulter, USA).

As for the qualitative analysis,  $1 \times 10^5$  cells were seeded on gelatin coated cover slip in 6-well plates and allowed to culture for 24 h. After another 4 h incubation with CFPE-labeled liposomes, cells were washed twice with cold PBS, fixed with 4% paraformaldehyde for 30 min, and stained with DAPI for 5 min. Finally, the cells were imaged using a confocal laser scanning microscopy (FV1000, Olympus, USA).

### C6 tumor spheroid uptake

C6 tumor spheroids *in vitro* were cultured as follows. Briefly, 2% (w/v) low melting point agarose was added into a 96-well plate.  $5 \times 10^3$  C6 cells were seeded on the agarose coated plate and incubated till uniform spheroids formed. CFPE-labeled liposomes were added for 4 h spheroids uptake, and then the spheroids were washed twice with cold PBS and imaged with a confocal microscopy (FV1000, Olympus, USA).

### BBB model study in vitro

BBB model was established using Millicell Hanging Cell Culture Inserts. In brief,  $1 \times 10^6$  bEnd.3 cells were plated into a cell culture insert and cultured for about 7 days. bEnd.3 monolayer with a transendothelial electric resistance (TEER) over 200  $\Omega$  could be used for further experiments. Then the cell culture inserts with bEnd.3 monolayer were transferred onto another 6-well plate containing pre-plated C6 cells and the whole system was co-cultured for another 24 h. CFPE-labeled liposomes were added into the donor chamber. After 8 h incubation, both bEnd.3 cells and C6 cells were collected and analyzed with a flow cytometer (Cytomics FC 500, Beckman Coulter, USA). On the other hand, C6 cells from the acceptor chamber were also imaged with a confocal microscopy (FV1000, Olympus, USA) for qualitative evaluation.

To identify the tight junction formed on the bEnd.3 monolayer, an immunofluorescence study was carried out. The bEnd.3 monolayer was incubated with Rabbit anti-mouse ZO-1 antibodies and followed by staining with FITC-labeled Goat anti-Rabbit secondary antibodies. Then the monolayer was washed with cold PBS, fixed and stained with DAPI, and finally imaged using a confocal microscopy (FV1000, Olympus, USA).

### Cytotoxicity and apoptosis study in vitro

C6 cells were plated in a 96-well plate at a density of  $2 \times 10^3$  cells per well for MTT assay. After cultured for 24 h, PTX-loaded liposomal formulations were added at pre-determined PTX concentrations for another 24 h incubation. 20  $\mu$ L MTT solution (5 mg/mL) was then added in each well for 4 h incubation. Finally, the medium was removed and the cells were dissolved in 150  $\mu$ L dimethyl sulfoxide. The ab-

sorbance of the solution was determined at 490 nm with a microplate reader (Thermo Scientific Varioskan Flash, USA).

Annexin V-FITC/PI dual staining was used for apoptosis study. C6 cells were treated with different groups of PTX-Lip or free PTX at a PTX concentration of 1  $\mu\text{g}/\text{mL}$ . After 24 h incubation, cells were collected, washed twice with cold PBS, suspended in 0.5 mL binding buffer and dual stained by Annexin V-FITC/PI. Finally, C6 cells were measured by a flow cytometer (Cytomics FC 500, Beckman Coulter, USA).

### Destruction of Vasculogenic Mimicry channels

*In vitro* VM formation was tested using a Matrigel-based tube formation assay. 150  $\mu\text{L}$  Matrigel was plated into 24-well plates and allowed to incubate for 1 h under 37 °C. C6 cells were resuspended with serum free culture medium and seeded on Matrigel at a density of  $2.5 \times 10^5$  cells per well. Different PTX-Lip or free PTX were added into the wells immediately to form a 1  $\mu\text{g}/\text{mL}$  PTX final concentration. After incubation for 6 h and 24 h, the plates were observed to monitor the formation of VM channels and photographed with Carl Zeiss 40CFL Axiovert 40 inverted microscopy (Germany).

### Cytotoxicity study on brain cancer stem cells

BCSCs were cultured following a previously described protocol. Briefly, C6 glioma cells were cultured with serum free DMEM culture medium containing 2% B27 supplement, 20 ng/mL basic fibroblast growth factor and 20 ng/mL epidermal growth factor. After continuous culture for 3 weeks, brain cancer stem cell tumorspheres were imaged with Carl Zeiss 40CFL Axiovert 40 inverted microscopy (Germany). Western blot was used for the detection of CD133 expression level. Total protein of C6 cells and C6 stem cells were resolved on 10% SDS-PAGE and transferred to polyvinylidene difluoride membranes. The membranes were incubated with Rabbit anti-CD133 primary antibodies, followed by incubation with HRP-labeled goat anti-rabbit secondary antibodies and finally detected by Immobilon Western HRP Substrate (Millipore, USA) on a Bio-Rad ChemiDoc MP System (Bio-Rad Laboratories, USA).

The induced C6 stem cells were suspended with serum containing culture medium again and seeded in 96-well plates at a density of  $2 \times 10^3$  cells per well. Cells were then treated as described above for MTT assay.

### In vivo imaging study

Balb/c mice were anesthetized and set on a stereotaxic apparatus. C6 glioma cells ( $1 \times 10^6$  cells/5  $\mu\text{L}$  in PBS) were slowly injected into the right brain of each mouse. After raised for about 10 days, glioma

bearing mice were injected with DiD-loaded liposomes. Mice were imaged with IVI Spectrum system (Caliper, Hopkington, MA, USA) at 1 h, 4 h, 8 h and 24 h after injection. Then the mice were sacrificed after heart perfusion and main organs including brains, hearts, livers, spleens, lungs and kidneys were collected. All the organs were imaged with IVI Spectrum system (Caliper, Hopkington, MA, USA). For liposomal glioma distribution, brains of the 24 h post-injection mice were fixed in 4% paraformaldehyde, dehydrated in 10% and 30% sucrose solution, and sectioned at the glioma domain at a thickness of 10  $\mu\text{m}$ . The sections were then incubated with DAPI for nuclei staining and imaged by a confocal microscopy (FV1000, Olympus, USA).

### Anti-glioma efficacy

C6 glioma bearing mice were randomly divided into 7 groups ( $n = 10$ ) as follows: Saline, free PTX, PTX-PEG-Lip, PTX-R8-Lip, PTX-R8-RGD-Lip, PTX-R8-EGR-Lip and PTX-R8-dGR-Lip. At 4, 6, 8, 10, 12 and 14 days after glioma inoculation, mice were intravenously injected with corresponding PTX formulations at a PTX dosage of 3 mg/kg. Saline group was used as negative control. On the 15<sup>th</sup> day of glioma implantation, one mouse of each group was chosen and sacrificed. All the seven brains were collected for paraffin sections. Hematoxylin and eosin (HE) staining was performed for tumor tissue observation. CD34 and periodic acid-Schiff (PAS) dual staining was used for VM monitoring, and CD133 based immunoperoxidase method was carried out for BCSCs observation. The survival time of the rest of the mice was recorded and Kaplan-Meier survival curves were plotted for each group.

### Statistical analysis

All the data were presented as mean  $\pm$  standard deviation. Statistical comparisons were performed by analysis of variance (ANOVA) for multiple groups, and  $p$  value  $< 0.05$  and  $< 0.01$  were considered indications of statistical difference and statistically significant difference respectively.

## Results and discussions

### Characterization of liposomes

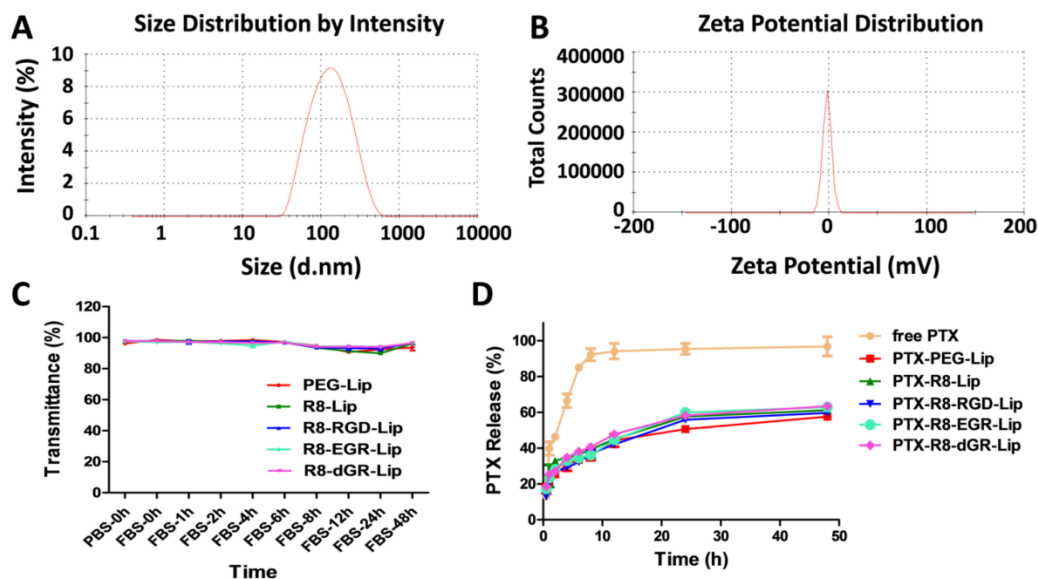
In order to prove the dual receptor recognizing ability of R8-dGR, three other peptides (R8, R8-RGD and R8-EGR) were utilized herein as controlled peptides. The CPP R8 without a specific binding motif was used as negative control. R8-RGD had an integrin  $\alpha_v\beta_3$  binding motif but couldn't recognize NRP-1 receptor without a CendR sequence while R8-EGR was just opposite. The observed molecular weights in the mass spectra of DSPE-PEG<sub>2000</sub>-R8-dGR,

DSPE-PEG<sub>2000</sub>-R8-RGD, DSPE-PEG<sub>2000</sub>-R8-EGR and DSPE-PEG<sub>2000</sub>-R8 were 4673, 4631, 4656, and 4308, respectively (See Supplementary Materials **Fig. S1-S4**) while the corresponding theoretic molecular weights of the four materials were 4640, 4640, 4654, 4312. Liposomes with average sizes between 100 nm and 120 nm and polydispersity index (PDI) less than 0.3 were prepared (See Supplementary Materials **Table S1**). It could be seen that the modification of R8 containing peptide made the liposomes less negative charged due to the electropositivity of polyarginine. PTX could be successfully loaded into the liposomes with entrapment efficiency (EE%) above 90%. The size and zeta potential distribution graphs of PTX-R8-dGR-Lip were shown in **Fig. 2A** and **Fig. 2B**. No aggregation was observed after 48 h liposomal incubation with FBS (**Fig. 2C**), indicating the satisfactory serum stability of different liposomes. The PTX release properties were determined through a dialysis method. The results showed that PTX-loaded liposomes exhibited a sustained drug release behavior over 48 h while free PTX carried out a rapid release in the media within 8 h (**Fig. 2D**). No significant difference was observed among all groups of liposomes.

### Surface plasmon resonance (SPR) analysis

The surface binding of drug delivery systems on cell membranes was considered as the first step of cellular uptake[27]. Thus the evaluation of the interaction efficiency between carriers and proteins on cell membranes was important for nanocarriers, especially for specific ligand modified ones. In this study, we utilized a reversed dGR peptide to create a CendR motif in the tandem peptide. Thus it is necessary to verify whether the sequence reversal would influence

the integrin binding activity of RGD. Herein, SPR analysis was carried out to investigate the specific binding ability of R8-dGR-Lip to integrin  $\alpha_v\beta_3$ . SPR is an optical method for detecting the molecular interaction by real-time measuring the refractive index between the samples and the sensor surface, and is widely used for evaluating the binding efficiency between ligands and receptor proteins[28-30]. In this study, integrin  $\alpha_v\beta_3$  was linked on the sensors and different modified liposomes were allowed to flow over the proteins. According to the recorded real-time response (RU) signal of different liposomes (**Fig. 3**), the response signal of PEG-Lip was close to baseline while the signal of R8-Lip increased a little probably resulting from the electronic interaction between positively charged arginine and negatively charged proteins. R8-EGR couldn't increase the liposomal interaction efficiency with integrin  $\alpha_v\beta_3$  compared to R8-Lip. In contrast, R8-RGD and R8-dGR significantly elevated the binding ability due to the addition of RGD or dGR in the sequence of R8 peptide. In fact, the peptide dGR came from a cyclic (vfdGR) peptide of which the integrin binding ability had been proved[31]. The dGR was an isomer of RGD peptide in which the direction of the sequence was reversed and the chirality of the aspartate residue was inverted. This class of isomers was called retro-inverso peptides[32], which would present an orientation of their side chains very similar to that of the original structure and have equal or even higher bioactivities compared to the parent peptides[33]. On this basis, we hypothesized the linear dGR would specifically recognize integrin  $\alpha_v\beta_3$  receptor as well and the SPR analysis results confirmed this conjecture.



**Fig. 2.** Characterization of liposomes. Size distribution graph (A) and Zeta potential distribution graph (B) of PTX-R8-dGR-Lip were measured by Malvern Zetasizer Nano ZS90. (C) The variations of transmittance of liposomes in 50% FBS over 48 h (n = 3, mean  $\pm$  SD). (D) PTX release behaviors of PTX-loaded liposomes and free PTX in release media for 48 h (n = 3, mean  $\pm$  SD).

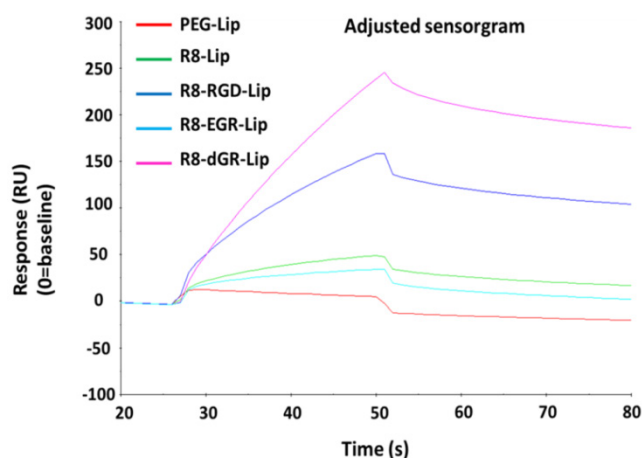


Fig. 3. SPR response curve of different modified liposomes with integrin  $\alpha_5\beta_3$ .

### Receptor expression level

The expression level of NRP-1 and integrin  $\beta_3$  receptors were detected on three cell lines by western blot study (Fig. 4A). As a receptor of vascular endothelial growth factor (VEGF) which regulates the vascular development and tumorigenesis, NRP-1 was usually considered to be overexpressed on both en-

dothelial cells and tumor cells[11, 34, 35]. Herein, NRP-1 was found expressed on all the three cell lines. On the other hand, integrin  $\beta_3$  was found expressed on both C6 cells and bEnd.3 cells but not on HeLa cells as we reported before[18]. The semi-quantitative evaluation of western blot of NRP-1 and integrin  $\beta_3$  was carried out using ImageJ and the results were shown in Supplementary Materials Fig. S6.

### Cellular uptake study

Receptor-mediated endocytosis is one of the most important mechanisms through which nanoparticulate carriers can overcome the obstacle of BBB and blood brain tumor barrier (BBTB)[36-38]. Thus liposomal uptake was evaluated on these three cell lines as well. Due to the existence of cell penetrating peptide, every R8 containing liposomal group exhibited an enhanced uptake capability compared to the conventional PEG-Lip. On glioma C6 cells and brain endothelial bEnd.3 cells which expressed both neuropilin-1 and integrin  $\alpha_5\beta_3$  receptors, R8-RGD and R8-EGR both significantly increased the cellular uptake of CFPE-labeled liposomes compared to R8-Lip (Fig. 4B).

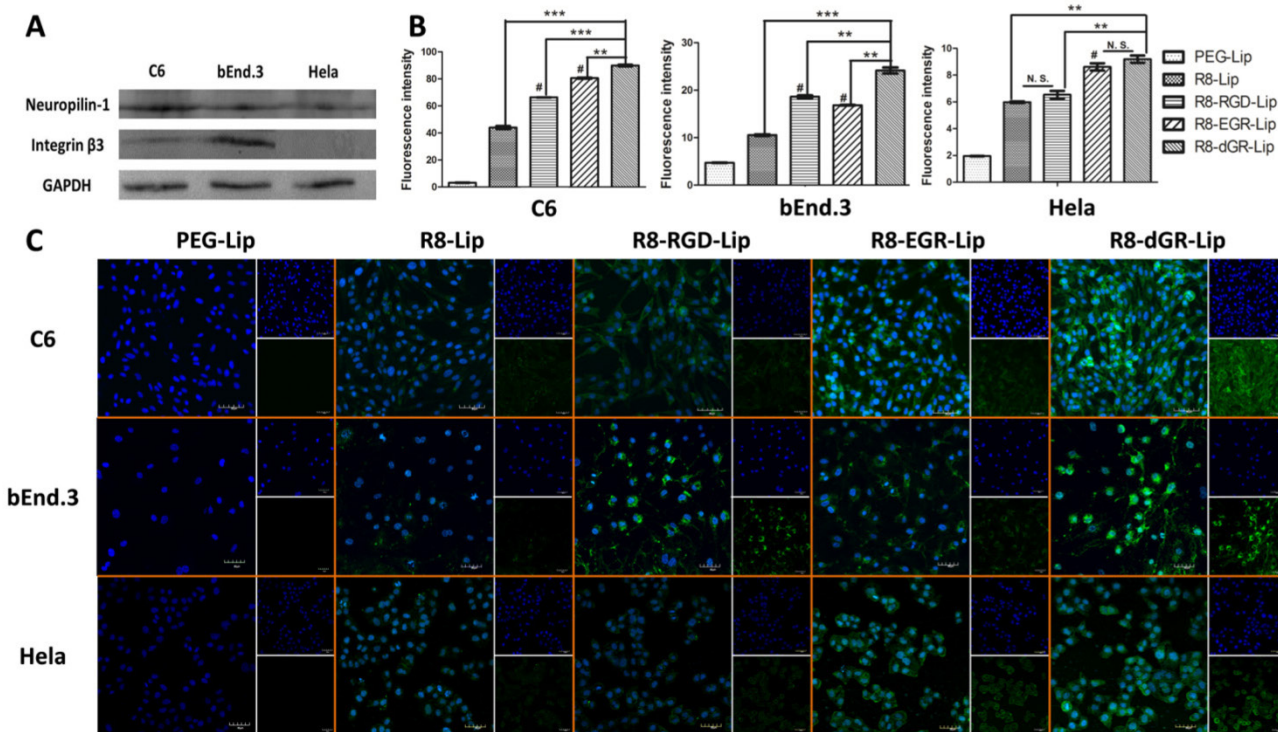


Fig. 4. (A) Expression level of Neuropilin-1 and integrin  $\beta_3$  on C6, bEnd.3 and HeLa cells. (B) Quantitative 4 h cellular uptake of CFPE-labeled liposomes on C6, bEnd.3 and HeLa cells determined by a flow cytometer ( $n = 3$ , mean  $\pm$  SD). \*\* and \*\*\* indicates  $p < 0.01$  and  $p < 0.001$  respectively, # represents  $p < 0.05$  versus R8-Lip group. (C) Confocal images of 4 h cellular uptake of CFPE-labeled liposomes on C6, bEnd.3 and HeLa cells.

According to the quantitative data, the addition of RGD in the sequence of R8 peptide increased the uptake of R8-Lip by 1.50-fold on C6 cells and 1.77-fold on bEnd.3 cells, while EGR-Lip increased the R8-modified liposomal uptake on C6 cells and bEnd.3 cells by 1.83-fold and 1.59-fold respectively. Interestingly, the difference in the uptake enhancement was completely corresponding with the disparity of receptor expression level on different cells. Thus we found that the enhancement of liposomal uptake induced by these tandem peptides was highly dependent on the receptor expression level. Meanwhile, R8-dGR-Lip exhibited the strongest internalization ability among all the liposome groups, indicating the dual receptor recognizing ability of R8-dGR. On the other hand, the cellular uptake on Hela cells between R8-Lip and R8-RGD-Lip didn't show significant difference because of the negative expression of integrin  $\alpha_v\beta_3$ . The same phenomenon was found between R8-EGR-Lip and R8-dGR-Lip. However, liposomal uptake was significantly enhanced while the CendR motif was added to the peptide sequence, which further proved the dual receptor dependent endocytosis property of R8-dGR-Lip. Confocal images in Fig. 4C exhibited the same results as described above in which strongest green fluorescence was observed in R8-dGR-Lip group on C6 cells and bEnd.3 cells, indicating R8-dGR as a potential ligand for BBB and glioma targeting.

### C6 tumor spheroid uptake

Three-dimensional tumor spheroids were usually used to mimic a number of native tumor environments including extracellular matrix, tumor macrostructure, and diffusion gradients[39, 40]. Thus tumor spheroid models were established herein to evaluate tumor penetrating ability of liposomes *in vitro*. C6 spheroids with diameters of 300-400  $\mu\text{m}$  were cultured with CFPE-labeled different modified liposomes for 4 h and R8-dGR-Lip exhibited the strongest internalization within the spheroids among all the groups (Fig. 5). Green fluorescence signal of R8-dGR-Lip could be observed till 200  $\mu\text{m}$  of the tumor spheroids while the penetrating depth of R8-RGD-Lip and R8-EGR-Lip was about 150  $\mu\text{m}$  and about 100  $\mu\text{m}$  for R8-Lip. Cell penetrating peptides were usually reported to mediate an enhanced intratumoral diffusion process of drug delivery systems[5, 41]. In this study, the penetration and diffusion of liposomes into avascular regions was further elevated when a specific receptor recognizing domain was added to the peptide sequence. For R8-RGD-Lip, the result is similar to our previously published work. The tumor targeting sequence RGD improved the tumor internalization and penetrating ability through the binding to integrin  $\alpha_v\beta_3$ . The penetrating of R8-EGR-Lip was even deeper than R8-RGD-Lip as Cend Rule could induce a stronger penetrating behavior than integrin  $\alpha_v\beta_3$ . And these results demonstrated the promise of a R8-dGR modification strategy for intratumoral penetration.

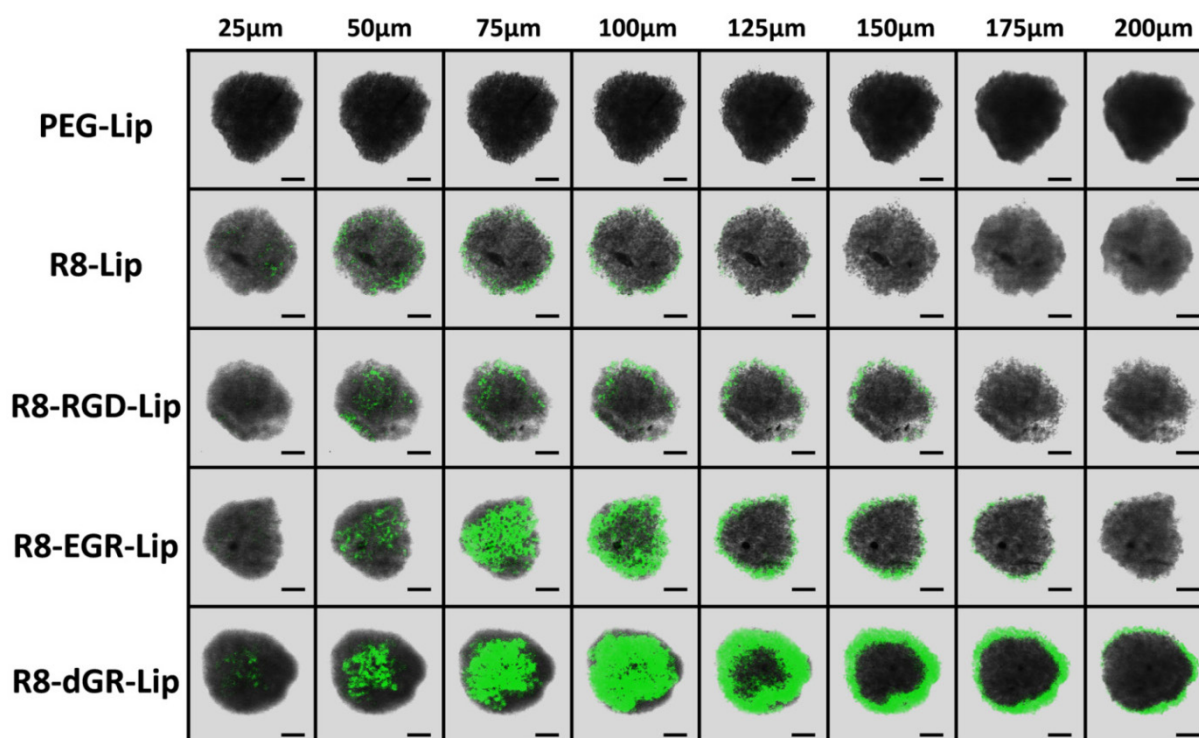
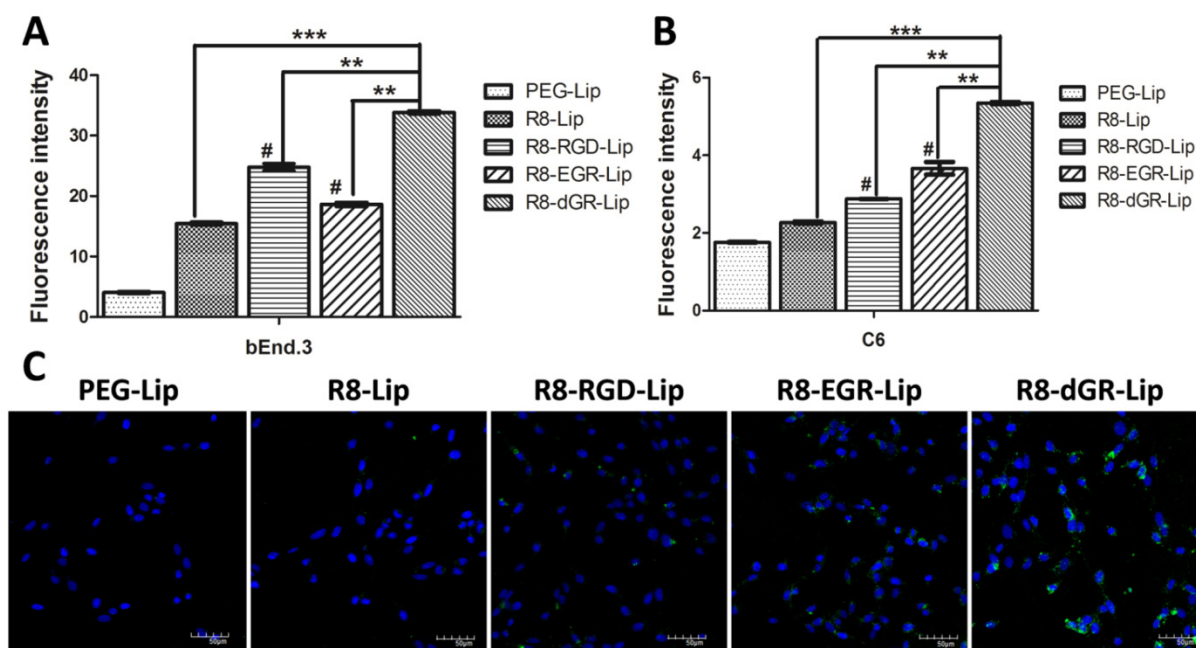


Fig. 5. Confocal images of the uptake of CFPE-labeled liposomes on C6 tumor spheroids with different depth. Scale bars represent 100  $\mu\text{m}$ .





**Fig. 6.** BBB model study *in vitro*. Uptake of CFPE-labeled liposomes on bEnd.3 cells on the transwell membrane (A) and on C6 cells in the presence of bEnd.3 monolayers (B) determined by a flow cytometer ( $n = 3$ , mean  $\pm$  SD), \*\* and \*\*\* indicates  $p < 0.01$  and  $p < 0.001$  respectively, # represents  $p < 0.05$  versus R8-Lip group. (C) Confocal images of the liposomal uptake on C6 cells in the presence of bEnd.3 monolayers.

### BBB model study *in vitro*

Transwell models were used to investigate the BBB transporting ability of different modified liposomes *in vitro*. A bEnd.3 monolayer/C6 co-culture model was utilized here. Effective glioma targeting drug delivery systems were expected to penetrate across the bEnd.3 monolayer and achieve efficient cellular uptake on C6 cells in the co-culture model. Thus the cellular uptake study on bEnd.3 cells in the donor chamber and on C6 cells in the acceptor chamber were both carried out. As shown in **Fig. 6A**, the uptake tendency of different liposomes on bEnd.3 monolayer was almost the same as that of the conventional liposomal uptake on bEnd.3 cells in **Fig. 4B**, indicating a normal internalization process of each group of liposomes on bEnd.3 monolayers from the Transwell membrane. After penetrating across the bEnd.3 monolayer, on the other hand, R8-dGR-Lip exhibited the highest uptake on C6 cells as well (**Fig. 6B**). Compared to the cellular uptake results on C6 cells in **Fig. 4B**, it could be found that the global uptake degree of every group of liposomes was greatly decreased due to the presence of the bEnd.3 monolayer. However, the enhanced percentage of cellular uptake of R8-dGR-Lip compared to R8-RGD-Lip and R8-EGR-Lip was even higher than the conventional liposomal uptake on C6 cells in **Fig. 4B**. These data confirmed the strongest BBB penetrating capability of R8-dGR compared to the other peptides. Confocal images in **Fig. 6C** supplied a same result as the quantitative data, in which the strongest uptake on C6 cells

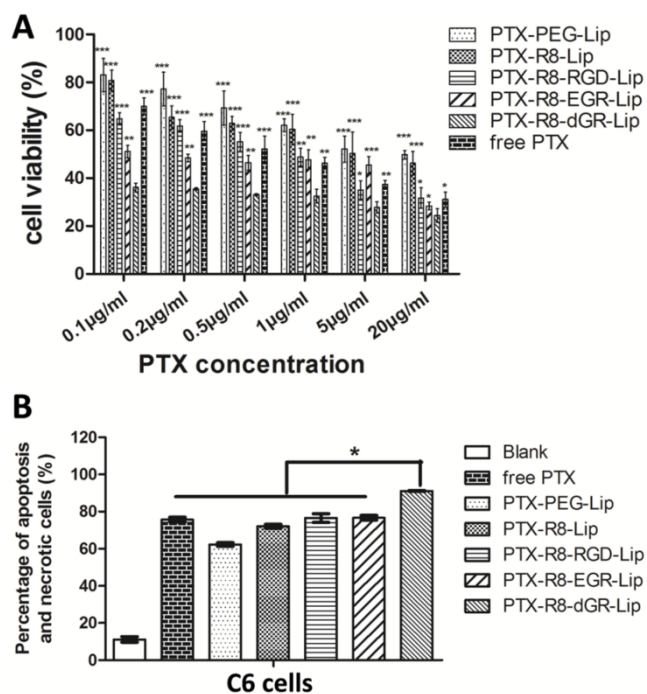
of R8-dGR-Lip in the presence of BBB model could be clearly observed.

An immunofluorescence analysis was also carried out to confirm the formation of tight junction on bEnd.3 monolayer. Zonula occludens protein 1 (ZO-1) is one of the ubiquitous molecular constituents of tight junctions, and it is commonly used for the identification of tight junction on the blood-brain barrier[42, 43]. As shown in **Fig. S7**, ZO-1 was stained with anti-ZO-1 antibody and was shown in green. The green fluorescence signal between the bEnd.3 cells indicated that tight junction was successfully formed.

### Cytotoxicity and apoptosis study *in vitro*

MTT study denoted the cytotoxicity of different liposomes on C6 glioma cells. As could be observed in Supplementary Materials **Fig. S8**, blank liposomal vehicles displayed satisfactory biocompatibility with all the cell viabilities over 85% after incubation with C6 cells for 24 h while the solvent of free PTX (ethanol-cremophor ELP 35 mixture, v/v = 1: 1) showed an inhibition as the concentration increased. As for the PTX-loaded liposomes, the MTT assay suggested that the anti-proliferation effect was PTX concentration dependent (**Fig. 7A**). PTX-loaded R8-RGD-Lip and R8-EGR-Lip displayed increased anti-proliferation effect compared to R8-Lip and conventional PEG-Lip, and PTX-R8-dGR-Lip exhibited the strongest inhibition effect among all the PTX formulations, even stronger than free PTX. Free drugs were usually used as positive controlled group in cytotoxicity study because they could be delivered into cells directly by

passive diffusion[44, 45], while drug carriers would inevitably undergo a sustained drug release process (Fig. 2D). Thus the MTT study confirmed that R8-dGR could most notably promote the cellular endocytosis of PTX-loaded liposomes. The IC<sub>50</sub> values of different PTX formulations were listed in Supplementary Materials Table S2. On the other hand, Annexin V/PI dual staining was utilized to carry out the apoptosis study. The cellular apoptosis dot diagrams of C6 cells after incubation with or without different PTX formulations were shown in Supplementary Materials Fig. S9. The apoptosis and necrosis rates of C6 cells after treated with free PTX, PTX-PEG-Lip, PTX-R8-Lip, PTX-R8-RGD-Lip, PTX-R8-EGR-Lip and PTX-R8-dGR-Lip for 24 h were 75.65 ± 1.77%, 62.25 ± 1.48%, 72.05 ± 1.49%, 76.50 ± 3.25%, 76.65 ± 1.57% and 91.05 ± 0.35%, respectively (Fig. 7B). Therefore, based on all the cytotoxicity and apoptosis study, R8-dGR had proved the capability to induce a significant enhanced inhibition of glioma cellular growth.



**Fig. 7.** (A) The cytotoxicity study of different PTX formulations on C6 cells (n= 3, mean ± SD). \*, \*\* and \*\*\* represent  $p < 0.05$ ,  $p < 0.01$  and  $p < 0.001$  versus PTX-R8-dGR-Lip group, respectively. (B) The percentage of apoptosis and necrotic cells after different PTX formulations treatment (n= 3, mean ± SD), \* represents  $p < 0.05$  versus other groups.

### Destruction of VM channels

Matrigel based tube formation model was used to investigate the formation of vasculogenic mimicry channels *in vitro* as reported[24, 46]. VM describe a mechanism by which tumor cells, especially highly aggressive malignant tumor cells, can form vessel-like structures themselves and function as an alternative blood and nutrients transporting pathway[20, 46, 47].

Thus the evaluation of VM channels destruction *in vitro* with the treatment of different PTX formulations was necessary. Glioma cells were reported to display a high degree of plasticity, which made them capable to differentiate and form tube-like structures[46, 48, 49]. As shown in Fig. 8A, in control group without PTX treatment, C6 cells would start to aggregate and turn fascicular 6 h after plated onto the surface of Matrigel, and further form long and apparent tubular structures after 24 h incubation. When different PTX formulations were added to the culture medium, the formation of VM channels was obviously inhibited. Glioma cells could only exhibit the tendency to adjoin each other within 6 h and finally form disconnected tube analogues 24 hours later in the PTX-treated groups. However, in the PTX-R8-dGR-Lip group, the cells always displayed scattered distribution instead of aggregation, and the formation of VM channels was interrupted. This destructive effect might be resulting from the cytotoxicity of PTX-loaded R8-dGR-Lip against C6 glioma cells, and the inhibition effect of VM formation *in vivo* was further addressed in the following pharmacodynamics study.

### Characterization and Cytotoxicity study of brain cancer stem cells

Cancer stem cells were usually correlated with drug resistance and relapse of malignant tumors[26]. Thus brain cancer stem cells were cultured and the cytotoxicity of liposomes on them was evaluated here. BCSCs were cultured and identified through both morphological observation and phenotypical detecting as reported[25]. After continuous culture in serum free culture medium for 3 weeks, BCSCs would present as suspended mammospheres under a microscope[22, 25]. As shown in Fig. 8B, the tumor spheres of C6 stem cells exhibited uniformly at diameters of about 50-100 µm. Meanwhile, the inherent nature of cancer stem cells was the positive expression of Prominin-1 (CD133) which was related to the tumorigenic potential of CSCs[19, 25]. Thus the expression level of CD133 on C6 glioma cells and the cultured C6 stem cells was detected here using western blot study. The CD133 expressed on C6 stem cells was obviously increased compared to normal C6 glioma cells (Fig. 8C), indicating that BCSCs were successfully formed in serum free culture medium. The semi-quantitative evaluation of western blot of CD133 was carried out using ImageJ and the result was shown in Supplementary Materials Fig. S10. Finally, the C6 stem cells were utilized to evaluate the cytotoxicity of PTX formulations on BCSCs *in vitro*. The results of MTT assay was shown in Fig. 8D. Compared to the cellular cytotoxicity on C6 glioma cells (Fig. 7A), it could be observed that the tolerance of the tumor stem cells to

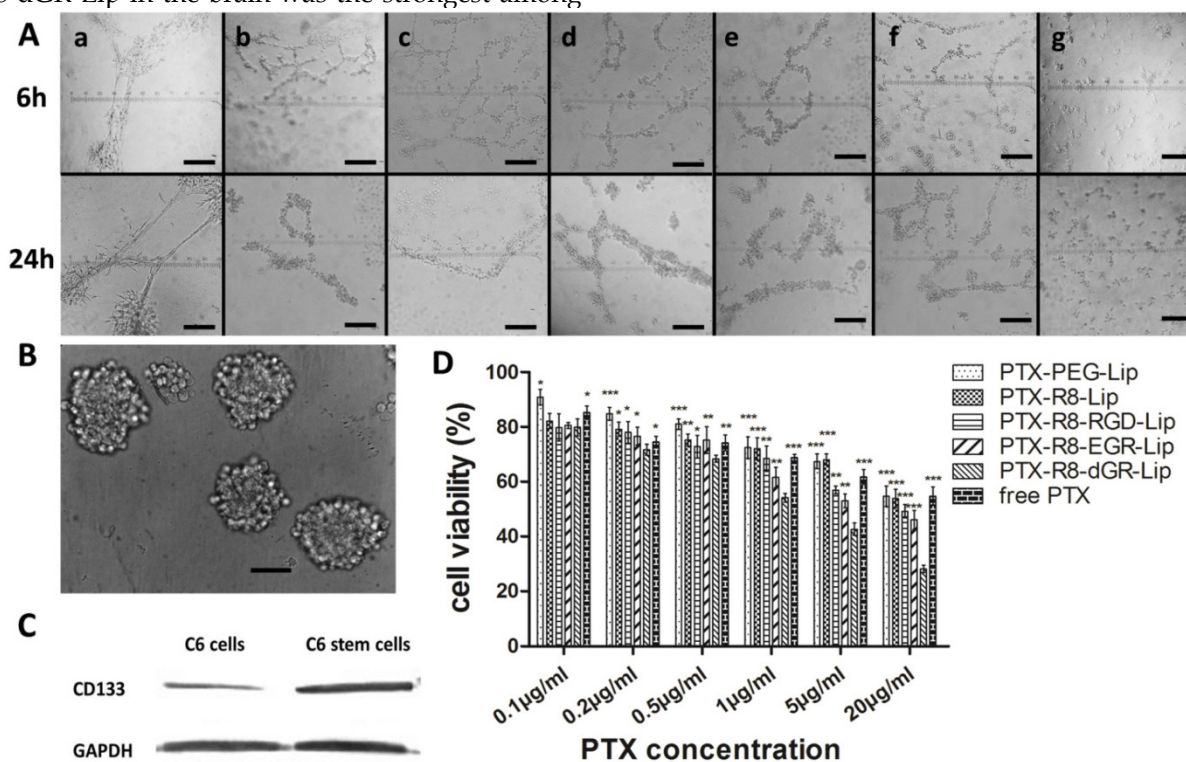
chemotherapeutics was significantly enhanced ( $IC_{50}$  values were listed in Supplementary Materials **Table S2**). All the C6 stem cells treated with PTX formulations with a concentration below 0.5  $\mu\text{g}/\text{mL}$  exhibited cell viabilities over 70%, which was due to the fact that cancer stem cells contribute to chemotherapy resistance[50, 51]. As the PTX concentration increased, the disparity between different modified liposomes became more significant. PTX-R8-dGR-Lip displayed a remarkable enhanced cytotoxicity to C6 stem cells compared to the other groups, which might be due to the improved internalization ability. All the *in vitro* experiments suggested the potential of R8-dGR modified liposomes as a drug delivery system for synthesized anti-glioma therapy.

### In vivo imaging and glioma distribution

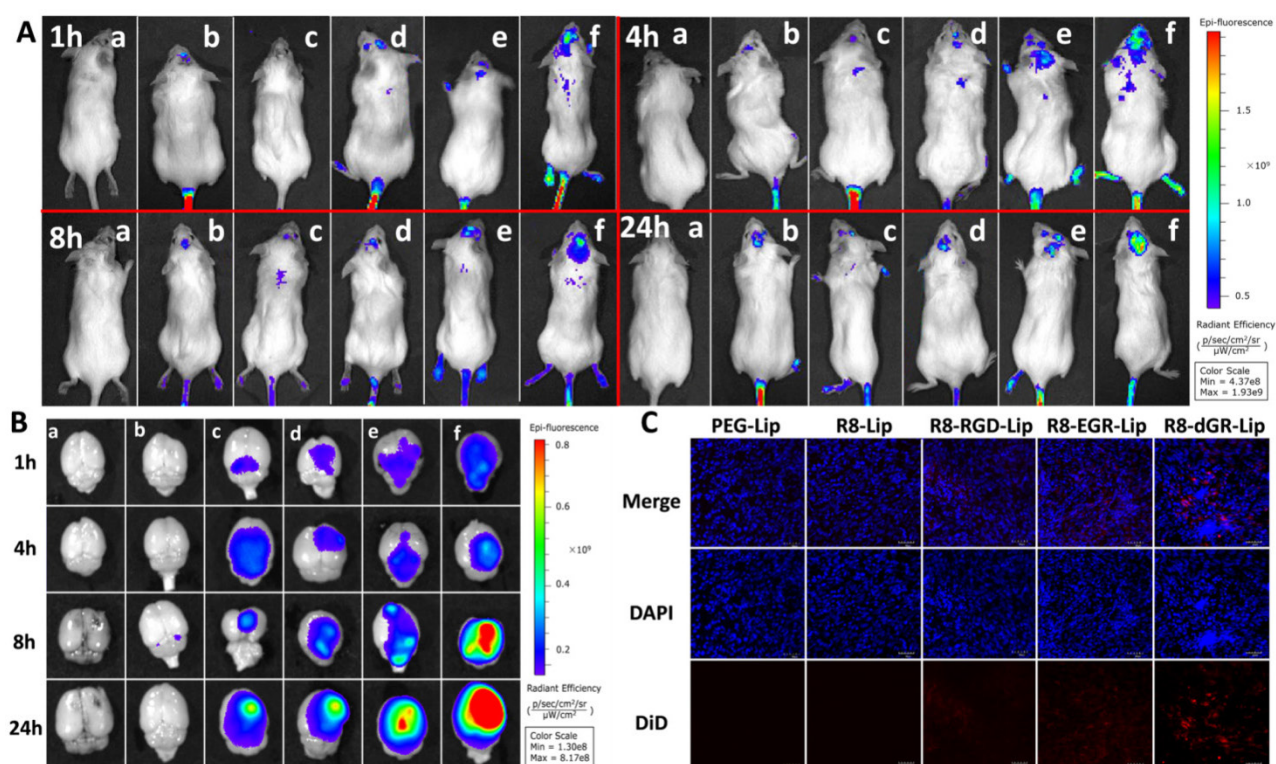
**Fig. 9A** and **Fig. 9B** displayed the *in vivo* images and *ex vivo* brains of C6 glioma bearing mice after systemic administration of different DiR-loaded liposomes. CPPs and specific ligands had both proved their advantages for BBB penetrating in many researches[52-55]. In this study, the tandem peptides (R8-RGD, R8-EGR and R8-dGR) could undergo both receptor-dependent and adsorptive-mediated BBB transporting process thus they exhibited increased brain delivery capabilities compared to R8 (**Fig. 9A**). And it could be observed that the fluorescence signal of R8-dGR-Lip in the brain was the strongest among

all the groups. Furthermore, as integrin  $\alpha_v\beta_3$  and NRP-1 receptors are overexpressed on both angiogenic tumor vessels and tumor cells[11, 56, 57], we suggested the dual recognizing tandem peptide R8-dGR could promote an active glioma targeting process and the results proved this hypothesis. The *ex vivo* brain images in **Fig. 9B** demonstrated that R8-dGR modified liposomes not only showed the strongest brain delivery, but also accumulated at the glioma foci most efficiently. Images of other organs were shown in Supplementary Materials **Fig. S11**.

Drugs must cross the vascular barrier and penetrate into the extravascular stroma to reach the inner tumor cells and tumor-associated parenchymal cells[58]. Therefore we then investigated the glioma distribution of the modified liposomes. According to the *in vivo* images, DiR-loaded liposomes achieved the highest accumulation at the glioma foci 24 h after systemic administration. Thus the brains of 24 h post-injection mice were sectioned and the inner glioma sites were imaged using a confocal microscope. Obvious red fluorescence signal was detected in the R8-dGR-Lip group (**Fig. 9C**), indicating an elevated accumulation and wide distribution of R8-dGR modified liposomes in the glioma tissue. The semi-quantitative results of the confocal images of glioma sections were analyzed using ImageJ and were shown in Supplementary Materials **Fig. S12**.



**Fig. 8.** (A) Destruction of C6 VM channels *in vitro* after 6 h and 24 h treatment of free PTX and PTX-loaded liposomes, untreated group was used as negative control. a = Saline, b = free PTX, c = PTX-PEG-Lip, d = R8-Lip, e = PTX-R8-RGD-Lip, f = PTX-R8-EGR-Lip, g = PTX-R8-dGR-Lip. Scale bars represent 200  $\mu\text{m}$ . (B) Morphological identification of C6 stem cell tumor spheres. Scale bar represents 50  $\mu\text{m}$ . (C) CD133 expression level on C6 cells and C6 stem cells. (D) The cytotoxicity study of different PTX formulations on C6 stem cells ( $n = 3$ , mean  $\pm$  SD). \*, \*\* and \*\*\* represent  $p < 0.05$ ,  $p < 0.01$  and  $p < 0.001$  versus PTX-R8-dGR-Lip group, respectively.



**Fig. 9.** (A) *In vivo* images of intracranial C6 glioma bearing mice at 1 h, 4 h, 8 h and 24 h post-injection of DiD-loaded liposomes. (B) *Ex vivo* images of the glioma bearing brains. In (A) and (B), a = blank, b = PEG-Lip, c = R8-Lip, d = R8-RGD-Lip, e = R8-EGR-Lip, f = R8-dGR-Lip. (C) Confocal images of glioma sections of C6 bearing mice 24 h after systemic administration of DiD-loaded liposomes.

Researchers suggested that CendR peptides would contribute to extravasation of the payload and penetration into tumor tissue through an NRP-1-binding pathway[58], and in this study it was proved that dual receptor recognizing ability would further enhance the progressive penetration. These *in vivo* results demonstrated that the dual receptor recognizing cell penetrating peptide R8-dGR possessed superior BBB transporting, glioma targeting and efficient tumor penetrating capabilities, and these properties would benefit the anti-glioma therapy effect of drug loaded liposomes.

### Anti-glioma efficacy

Kaplan-Meier survival curves (Fig. 10A) demonstrated a prolonged survival time of modified liposomes. The medium survival time glioma bearing mice treated with PTX-R8-dGR-Lip group (40 days) was significant longer than that of saline (19 days), free PTX (29 days), PTX-PEG-Lip (27 days), PTX-R8-Lip (29 days), PTX-R8-RGD-Lip (35 days) and PTX-R8-EGR-Lip (30 days) (Table 1). Then the synthesized anti-glioma therapeutic efficacy was evaluated through several staining of different glioma sections. Hematoxylin-eosin staining (HE staining) in Fig.10B exhibited large tracts of tumor tissue in the saline-treated group, while the color in PTX formulation treated groups was shallower. The most signifi-

cant reduction of glioma area was observed in the PTX-R8-dGR-Lip group, indicating an increased anti-proliferation effect of tumor cells induced by R8-dGR *in vivo*. On the other hand, CD34-PAS dual staining was used for detecting VM channels *in vivo*. CD34 was used to mark endothelial and endothelial progenitor cells while PAS could stain vascular basement membranes[21, 46]. Therefore, the non-endothelial tumor cell-lined VM microvascular channels would be PAS-positive and CD34-negative and reflect as pink tubes. Fig. 10C demonstrated obvious decrease of VM channels in the PTX-R8-dGR-Lip group while long and clear tubular structures were observed in other groups. As VM channels functioned as an alternative blood supply network, the destruction of VM could cut off the nutrients transporting and contribute to an enhanced anti-tumor effect, especially to the aggressive malignant tumors[59, 60]. Finally, CD133 immuno histochemical staining was carried out to identify BCSCs. As shown in Fig. 10D, a crowd of CD133 positive cancer stem cells stained in brown was observed in saline group. After treatment of PTX formulations, stem cells were decreased in different degrees. However, CD133 negative cells shown in blue were observed instead in the R8-dGR modified liposome group, indicating the most efficient anti-cancer stem cells effect of PTX-R8-dGR-Lip. Meanwhile, we had

detected the expression level of integrin  $\alpha_v\beta_3$  and neuropilin-1 on C6 stem cells as well, and no significant difference was found between C6 cells and C6 stem cells (Data not shown). The only difference between C6 cells and BCSCs was the increase expression of CD133. Therefore, R8-RGD-Lip and R8-EGR-Lip could also achieve enhanced toxicity to BCSCs through integrin and NRP-1 mediated cellular internalization respectively. In conclusion, PTX-loaded liposomes decorated with the dual receptor recognizing peptide R8-dGR displayed an efficient synthesized anti-glioma effect including anti-tumor cells, anti-VM and anti-BCSCs, which would probably lead to an exhaustive therapeutic efficacy and prevention of glioma relapse.

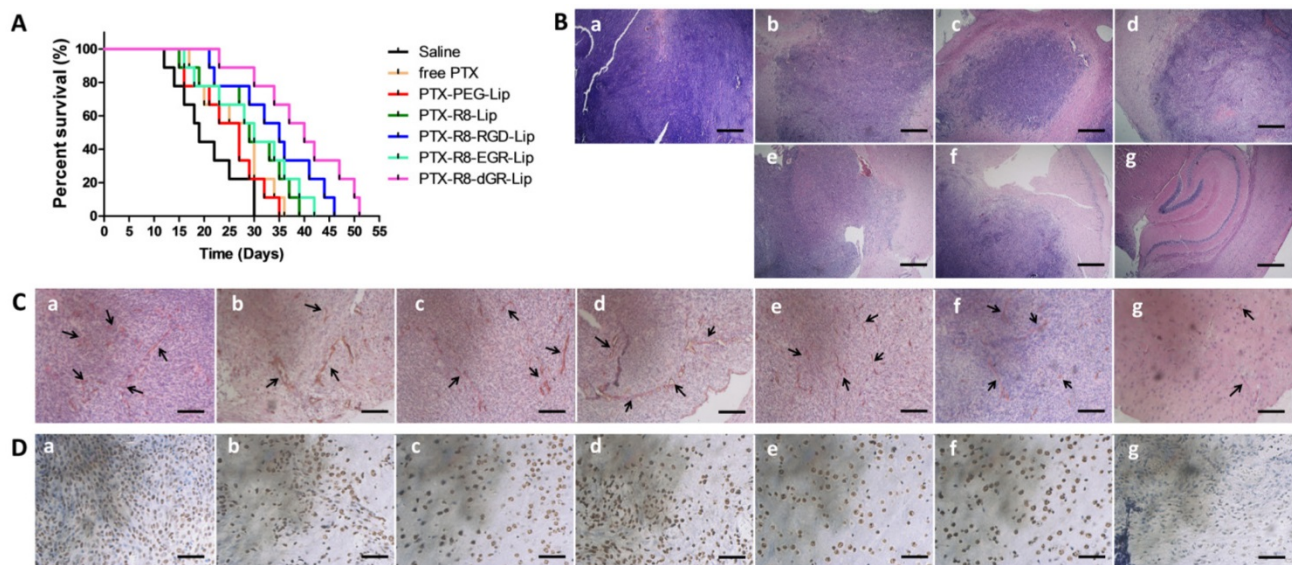
## Conclusion

In this study, we have designed a PTX-loaded liposomal drug delivery system modified with a tandem peptide R8-dGR. As a dual receptor recognizing cell penetrating peptide, R8-dGR displayed strong BBB transporting, glioma targeting and penetrating

capabilities. Based on these properties, PTX-R8-dGR-Lip exhibited synthesized anti-glioma therapeutic effects including anti-tumor cells, anti-VM and anti-BCSCs. Therefore, we suggested the R8-dGR modified liposomes as a potential drug delivery system for anti-tumor therapy.

**Table 1.** The median survival time of the glioma bearing mice treated with different PTX formulations (*a**p* < 0.05 versus Saline, *b**p* < 0.05 versus free PTX, *c**p* < 0.05 versus PTX-PEG-Lip, *d**p* < 0.05 versus PTX-R8-Lip, *e**p* < 0.05 versus PTX-R8-RGD-Lip, *f**p* < 0.05 versus PTX-R8-dGR-Lip).

Group	Median (day)	Standard error	95% confidence interval	Significant	Increased survival time
Saline	19	2.2	16.3-24.9	--	--
free PTX	29	2.3	22.2-31.1	a	53%
PTX-PEG-Lip	27	2.3	20.5-29.5	a	42%
PTX-R8-Lip	29	2.7	23.8-34.4	a	53%
PTX-R8-RGD-Lip	35	3.0	28.2-39.8	a,b,c,d	84%
PTX-R8-EGR-Lip	30	3.0	23.6-35.5	a	58%
PTX-R8-dGR-Lip	40	3.1	33.2-45.5	a,b,c,d,e,f	110%



**Fig. 10.** The anti-glioma assay of PTX-loaded liposomes on intracranial C6 bearing mice. (A) Kaplan-Meier survival curve of intracranial C6 glioma bearing mice treated with different PTX formulations (*n* = 9). Saline group was used as negative control. Red arrows indicate times of treatment. (B) HE staining of brain glioma tissues. Scale bars represent 400  $\mu$ m. (C) CD34-PAS dual staining of brain glioma tissues. Scale bars represent 200  $\mu$ m. Black arrows indicate pink vasculogenic mimicry *in vivo*. (D) CD133 staining of brain glioma tissues. Scale bars represent 50  $\mu$ m. Brain cancer stem cells with CD133 positive expression were shown in brown. In (B)-(D), a = Saline, b = free PTX, c = PTX-PEG-Lip, d = R8-Lip, e = PTX-R8-RGD-Lip, f = PTX-R8-EGR-Lip, g = PTX-R8-dGR-Lip.

## Supplementary Material

Figures S1- S12, Tables S1-S2.

<http://www.thno.org/v06p0177s1.pdf>

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## Abbreviations

CPP: cell penetrating peptide; BBB: blood-brain barrier; IFP: interstitial fluid pressure; NRP-1: neuropilin-1; VM: vasculogenic mimicry; BCSCs: brain cancer stem cells; PTX: paclitaxel; SPC: Soybean

phospholipids; CFPE: 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine-N-(carboxyfluorescein); HRP: horseradish peroxidase; DiD: 1, 10-dioctadecyl- 3, 3, 30, 30-tetramethylindodicarbocyanine, 4-chlorobenzenesulfonate salt; SPR: surface plasmon resonance; FBS: fetal bovine serum; TEER: transendothelial electric resistance; MTT: 3-(4,5-dimethylthiazol-2-yl)-2,5-diphenyltetrazolium bromide; PAS: periodic acid-Schiff; PDI: polydispersity index; EE: entrapment efficiency; VEGF: vascular endothelial growth factor; BBTB: blood brain tumor barrier; ZO-1: zonula occludens protein 1; CD133: prominin-1.

## Competing Interests

The authors have declared that no competing interest exists.

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